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(54) DISPOSABLE MODULAR HEARING AID

WEGWERFBARES MODULARES HÖRHILFEGERÄT

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(56) References cited:

EP-A- 0 782 371	WO-A-93/25053
GB-A- 2 155 276	US-A- 4 739 512
US-A- 4 834 211	US-A- 4 870 688
US-A- 5 185 802	

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EP 1 175 811 B1

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Description**BACKGROUND OF THE INVENTION**

[0001] Hearing aids are delicate electro-acoustical devices that are intended to perform flawlessly in the harsh environment of the human ear. Hearing aid manufacturers use hard durable earmold materials to protect the delicate electronics and transducers from adverse conditions in and out of the ear. Such durable materials are intended to survive a greater than four year usage life. The earmold can be used not only to protect the internal components of the hearing aid, but also to form an interface between the electronics and the ear canal. This interface must be created to prevent acoustical feedback, to retain the electronics in the ear and prevent irritation or fatigue of the ear canal. A design conflict for the earmold can then exist between the need to have a soft, pliant, nonirritating and comfortable material, and the need to have a durable material to protect the internal electronic components which can last more than four years.

[0002] A disposable hearing aid is one designed to have a useful life of much less than the traditional four years. The useful life of a disposable hearing aid can also be governed by the life of the battery. If the battery can be replaced, the hearing aid is no longer disposable and the advantages of the disposable aid are lost. However, a number of other variants on the disposable aid are possible. These variants look to maintain the advantages of disposability while making the system more convenient, comfortable, longer lasting or providing better performance.

[0003] "One-size-fits-all" type hearing aids generally lack a flexibility of their tips. Such a lack of flexibility prevents deep penetration into the bony region of an ear canal by the hearing aid. Such hearing aids are also unable to create an acoustic seal in the ear canal. Without such penetration or such a seal in the bony region, the hearing aid can create an occlusion effect in the wearer. Also, hearing aids lacking a proper acoustic seal are prone to feedback.

[0004] Feedback is a nagging, unsolved problem for hearing aid manufacturers and dispensers. Feedback in a hearing aid is present in several forms: electrical, acoustical and mechanical. While electrical feedback is more easily controllable with additional circuitry, the latter two forms of feedback in hearing aids remain significant problems that often reduce the effectiveness of hearing aid fittings. Acoustical or mechanical feedback signals from the hearing aid receiver may be transduced by the hearing aid microphone, amplified in the circuitry and output from the receiver again but with higher gain, creating a feedback loop, and potentially oscillation. A criterion by Nyquist states that a system will oscillate if the gain of the open loop transfer function at a particular frequency is greater than or equal to unity and its phase shift of the open loop transfer function is a multiple of

360 degrees. Acoustical feedback occurs through the air inside of the hearing aid housing as well as on the outside of the hearing aid while it is being worn. Mechanical feedback occurs because of the receiver vibrating

5 the hearing aid housing. Hearing aid designers have used many techniques to prevent the creation of such feedback loops. Included are rubber isolation mounts for the microphone and receiver, stiff tubes on the receiver output port and electronically filtering the hearing aid 10 output to suppress energy at the most likely to be troublesome feedback frequencies. Unfortunately, hearing aids frequently have feedback oscillation frequencies in the very range at which the wearer requires amplification most, such as in the frequency range between 1500 and 5000 Hz.

[0005] One possible solution to the conflict between comfort and durability of the earmold is the creation of a disposable hearing aid which uses ultra soft earmold 15 materials that may not last over a four year period, but 20 can be mass produced in an economically competitive manner. The earmold can therefore be replaced more frequently than the disposable hearing aid. An earmold that is replaced on a more frequent basis than the replacement cycle of the disposable aid can provide a user 25 with benefits. If the earmold is replaced on a daily basis, as compared to a base unit which is replaced after a much longer period of time than the earmold, the user can be provided with a high degree of comfort, cleanliness, and performance.

[0006] Earmold tip flexibility is necessary to allow for 30 deep ear canal insertion of a hearing aid to overcome the convolutions present in a typical ear canal. An earmold having a flexible tip incorporated with the earmold 35 can have several advantages. These advantages include potentially deep ear canal fittings, efficient coupling of the sound emitted from the receiver to the ear drum, and a corresponding reduction in the required output levels of the receiver. The flexible tip can also provide a comfortable fit even for cases where the tip is 40 located in the bony region of the ear canal. It is observed that when the tip creates a seal in this bony region, the occlusion effect is substantially mitigated.

[0007] The compliance of an earmold tip of a hearing 45 aid is also important in hearing aid design. If the earmold tip is compliant enough, the tip can fit into many different sizes and shapes of ear canals. A desirable tip is one that slides easily into the bony structure of the ear canal, feels comfortable and provides a good acoustic seal.

[0008] US-A-4,739,512 is prior art to this application. 50 US-A-4,870,688 discloses of the preamble of claim 1. The present invention is characterized by the features of the characterizing portion of claim 1. Optional features are recited in the dependent claims.

[0009] The flexible earmold tip for a hearing aid can 55 have a vibration isolator portion. A mushroom shaped tip portion for insertion into an ear canal and a sound bore can be formed between the vibration isolator portion and the mushroom shaped tip portion. The vibration

isolator portion includes a receiver having a diaphragm adapted to vibrate in operation creating acoustical vibrations which cause the receiver to mechanically vibrate. The vibration isolation portion attenuates such mechanical vibrations from the receiver. The vibration isolation portion mechanically decouples the receiver from a hearing aid base unit to isolate the mechanical vibrations of the receiver from the base unit.

[0010] The sound bore includes a spring and a compliant material surrounding the sound bore where the spring prevents collapsing of the sound bore and controls the flexibility of the flexible earmold tip. The flexible earmold tip includes an outlet port which allows collection of earwax without clogging the sound bore. The hearing aid, to which the flexible earmold tip is attached, includes a base unit in which is mounted a microphone. The mushroom shaped tip portion creates a seal with an ear canal to acoustically isolate a hearing aid base unit from acoustical vibrations created by the receiver. The vibration isolation portion can include a nest in which the receiver sits to acoustically seal the receiver within the vibration isolation portion thereby acoustically isolating the hearing aid base unit from the acoustical vibrations created by the receiver.

[0011] A hearing aid and tip assembly can include a hearing aid base unit having a microphone, a battery and electronics, and a flexible earmold tip having a vibration isolator portion, a mushroom shaped tip portion and a sound bore. The vibration isolator portion is enclosed by the base unit and includes a receiver electrically attached to the base unit where the receiver includes a diaphragm adapted to vibrate in operation causing the receiver to mechanically vibrate. The vibration isolation portion attenuates vibrations from the receiver. The mushroom shaped tip portion is attached to the vibration isolator portion. The sound bore is formed between the vibration isolator portion and the mushroom shaped tip portion and provides a channel for the transfer of sound from the receiver to an ear canal of a user.

[0012] The sound bore includes a spring and a compliant material surrounding the sound bore where the spring prevents collapsing of the sound bore and controls the flexibility of the flexible earmold tip. The flexible earmold tip can also include an outlet port which allows collection of earwax without clogging the sound bore. The vibration isolation portion can mechanically decouple the receiver from the base unit to isolate the mechanical vibrations of the receiver from the base unit. The mushroom shaped tip portion can create a seal with an ear canal to acoustically isolate the hearing aid base unit from acoustical vibrations created by the receiver. The vibration isolation portion comprises a nest in which the receiver sits to acoustically seal the receiver within the vibration isolation portion thereby acoustically isolating the base unit from acoustical vibrations created by the receiver.

[0013] Feedback can be attenuated within a hearing

aid by providing a hearing aid base unit, a receiver, and a hearing aid tip having a flexible mushroom shaped tip portion and vibration isolator portion. Surrounding the receiver with the vibration isolator portion attenuates

5 acoustic vibrations and mechanical vibrations created by the receiver during operation. Securing the vibration isolator portion and receiver within the hearing aid base unit further mechanically decouples the receiver from the base unit. Placing the hearing aid within an ear causes the mushroom shaped tip portion to form a seal with the ear canal to attenuate acoustic vibrations produced by the receiver.

BRIEF DESCRIPTION OF THE DRAWINGS

15 [0014] The foregoing and other objects, features and advantages of the invention will be apparent from the following more particular description of preferred embodiments of the invention, as illustrated in the accompanying drawings in which like reference characters refer to the same parts throughout the different views. The drawings are not necessarily to scale, emphasis instead being placed upon illustrating the principles of the invention.

25 Figure 1 illustrates an embodiment of a modular hearing aid having a replaceable earmold.

30 Figure 2 illustrates an alternate embodiment of the hearing aid of Figure 1, the hearing aid having a battery integral with an earmold.

35 Figure 3A shows an alternate arrangement of the hearing aid of Figure 1, which is not according to the present invention, the hearing aid having a battery and an earmold integral with a shell.

40 Figure 3B shows an alternate arrangement of the hearing aid of Figure 1, which is not according to the present invention, the hearing aid having a battery, a receiver and an earmold integral with a shell.

45 Figure 4A illustrates a hearing aid having an integral earmold and shell, which is not according to the present invention, the shell housing a receiver.

50 Figure 4B illustrates a hearing aid having an integral earmold and shell, the earmold housing a receiver, according to the present invention.

55 Figure 5 illustrates an alternate embodiment of the hearing aid of Figure 1, the hearing aid having a replaceable earmold integrated with a shell having a battery and receiver.

Figure 6 illustrates an alternate embodiment of the hearing aid of Figure 1, the hearing aid having a receiver incorporated with the earmold.

Figure 7 illustrates an alternate embodiment of the hearing aid of Figure 6.

Figure 8 illustrates an alternate embodiment of the hearing aid of Figure 1 where the replaceable earmold incorporates a portion of the shell.

Figure 9 shows an alternate arrangement of the hearing aid of Figure 1, which is not according to

the present invention, where the earmold allows the replacement of an integral shell and electronics module.

Figure 10 shows an alternate embodiment of the hearing aid of Figure 1 where the earmold allows the replacement of an integral shell, electronics and receiver module.

Figure 11 illustrates an alternate arrangement of the hearing aid of Figure 1, which is not according to the present invention where the hearing aid has a base unit, a replaceable shell module and a replaceable earmold integrated with a battery.

Figure 12 illustrates an alternate embodiment of the hearing aid of Figure 11.

Figure 13 shows an alternate arrangement of the hearing aid of Figure 11, which is not according to the present invention.

Figure 14 illustrates a top view of a flexible earmold tip for a hearing aid.

Figure 15 illustrates a side view of a flexible earmold tip for a hearing aid.

Figure 16 illustrates a front view of a flexible earmold tip for a hearing aid.

Figure 17 and 18 shows a cross-sectional view of a flexible earmold tip.

Figure 19 shows a cross-sectional view of a hearing aid having a flexible earmold tip as illustrated in Figures 14-16.

Figure 20 shows a hearing aid having a flexible earmold tip as illustrated in Figures 14-16.

Figures 21-24 illustrate a disposable hearing aid having a compliant tip, but which are not according to the present invention.

DETAILED DESCRIPTION OF THE INVENTION

[0015] An embodiment of a modular hearing aid 10 is shown in Figure 1. The modular hearing aid 10 can have an earmold 12 and a base unit 36. The base unit 36 can be a rigid or semi-rigid structure to which the earmold is attached or which holds and aligns other internal components. In one embodiment, the base unit 36 can be a core 14 having a shell 16. In a preferred embodiment both the earmold 12 and the base unit 36 can be replaced by the user after use. The earmold 12 can be replaced on a more frequent basis than the base unit 36.

[0016] The earmold 12 can have three preferred embodiments in any given embodiment of the modular hearing aid 10. In one embodiment, the earmold 12 forms an earmold tip 18. The earmold tip 18 can be made from an ultra soft and compliant material. The material can be an injection moldable, biocompatible thermoelastomer, such as C-flex (Consolidated Polymer Technologies, Inc., Largo, FL). The material, in a preferred embodiment, can be a castable, biocompatible silicone polymer, such as PlatSil (Polytek Development Corporation, Easton, PA). The earmold tip can also attach to a distal end of the shell 16 and extend into an

ear canal. In another embodiment, the earmold 12 forms an earmold sleeve 20. The earmold sleeve 20 can be made from an ultra soft and compliant material. The earmold sleeve 20 can also cover a portion or all of the base unit 36. In a third embodiment, as shown in Figure 1, the earmold 12 forms an earmold tip 18 and sleeve 20. In this embodiment, the tip 18 and sleeve 20 can be made from an ultra soft and compliant material. The tip 18 and sleeve 20 can also cover a portion or all of the shell 16 and can extend into the ear canal.

[0017] The earmold 12 can be formed such that it firmly holds onto the core 16 by a retention mechanism. The retention mechanism can be a mechanical snap, mechanical twist-lock or friction, for example.

[0018] The modular hearing aid 10 can also include a microphone, a receiver, electronics and controls. The electronics can include an integrated circuit and passive components. The controls can include an on-off control and a volume control. In one embodiment, these components are located within the core 14. The modular hearing aid can also have a battery.

[0019] In an alternate embodiment of the bearing aid with replaceable earmold 10, the earmold 12 can include a battery 22, as shown in Figure 2. The battery 22

integrated with the earmold 12 includes an electrical connection to the base unit 36. The battery 22 can include contacts 24 which connect to the core 14. In this embodiment, the earmold 12 and battery 22 are provided as a single unit, which is replaceable on the hearing aid core 14. Frequent replacement of the battery 22 and earmold 12 can provide a user with an optimum level of comfort, cleanliness performance and economy. Integrating the battery 22 with the earmold 12, the battery 22 can be more easily handled by the user because the integrated battery and earmold are larger than the battery alone.

[0020] The combined earmold 12 and battery 22 can form an ear mold tip 18, an ear mold sleeve 20 or an ear mold tip 18 and sleeve 20, similar to that described above. The earmold 12 and battery 22 can be retained on the core 14 by mechanical snap or friction, for example. The contacts 24 of the battery 22 can also be used to retain the combined earmold 12 and battery 22, to the core 14.

[0021] Figure 3A illustrates a modular hearing aid 10, not according to the present invention having a replaceable earmold 12, shell 15 and battery 22 formed as one integral unit. This unit can act as a covering for a hearing aid base unit. The battery 22 integrated with the earmold

12 includes an electrical connection to the base unit 36. The components of a hearing aid that can be replaced or are preferably replaced are the battery 22, the earmold 12 and the shell 15. The battery 22 can be replaced because batteries generally lose their powering ability after a certain amount of use. The earmold 12 and the shell 15 can be replaced because the components contacts the ear canal and can require frequent cleaning.

[0022] This modular hearing aid 10 can have a base

unit 36 which can include a microphone 30, electronics 28 and a receiver 26. The earmold 12 and shell 15 integral with the battery 22 can be mechanically or frictionally attached to the non-replaceable base unit 36. The base unit 36 can fit within the shell 15 for attachment. The battery 22 can have contacts 24 which can connect to the base unit 36. When the contacts 24 of the battery 22 are mated to the base unit 36, current can flow from the replaceable battery 22 to the electronics 28 in the base unit 36. The contacts 24 of the battery 22 can also be used to retain the integrated earmold 12 and battery 22 to the base unit 36.

[0023] Figure 3B illustrates another arrangement of the modular hearing aid 10, not according to the present invention, where the earmold 12 and shell 15 are integrated with a battery unit 22 and a receiver 26. In this embodiment, the hearing aid 10 can also have a base unit 36 having a microphone 30 and electronics 28. The battery 22 integrated with the earmold 12 includes an electrical connection to the base unit 36. In this embodiment the earmold 12, shell 15, battery 22 and receiver 26 are integrated into a single unit that can act as a covering for a base unit 36 and that the unit can be replaced more frequently than the base unit 36, which may or may not be disposable. This provides convenience, cleanliness and product longevity to the user.

[0024] The receiver 26 can be incorporated into the replaceable earmold 12 and shell 15 for two reasons. First, the receiver 26 is preferably placed deep into the ear canal in order to achieve the highest effective sound pressure levels possible. For many types of hearing aids, the earmold 12 also protrudes deeply in the ear canal to guide and position the electronics 28 and receiver 26. Therefore integrating the receiver with the earmold 12 and shell 15 allows placement of the receiver deep into the ear canal.

[0025] Second, the receiver 26 can be incorporated into the replaceable earmold 12 and shell 15 because it is very prone to damage if the modular hearing aid 10 is dropped from a height of several feet onto a hard surface. By integrating the receiver 36 with the replaceable earmold 12 and shell 15, replacement of a damaged receiver 36 is easily performed by a user. Being able to replace the receiver after damage can add longevity to the unit 10.

[0026] Figure 4A shows an arrangement of a modular hearing aid 10, not according to the present invention, having a replaceable earmold 12, shell 15 and receiver 26, formed as one unit, where the shell 15 houses the receiver 26. The unit can act as a covering for a hearing aid base unit. The components of a hearing aid that can be replaced or are preferably replaced are the receiver 26, the earmold 12 and the shell 15. The receiver 26 can be easily replaced by a user when the receiver 36 is damaged. The earmold 12 and the shell 15 can be replaced because the components contacts the ear canal and can require frequent cleaning.

[0027] This embodiment of the modular hearing aid

10 can have a base unit 36 which can include a microphone 30, electronics 28 and a battery 22. The earmold 12 and shell 15 integral with the receiver 26 can be mechanically or frictionally attached to the non-replaceable base unit 36. The base unit 36 can fit within the shell 15 for attachment. The receiver 26 can electrically connect to the base unit 36.

[0028] Figure 4B shows another embodiment of a modular hearing aid 10 having a replaceable earmold 12, shell 15 and receiver 26, formed as one unit, where the earmold 12 houses the receiver 26. The unit can act as a covering for a hearing aid base unit. Similar to the hearing aid 10 described above, the modular hearing aid 10 can have a base unit 36 which can include a microphone 30, electronics 28 and a battery 22. The earmold 12 having the receiver 26 and the shell 15 can be mechanically or frictionally attached to the non-replaceable base unit 36. The base unit 36 can fit within the shell 15 for attachment and the receiver 26 can electrically connect to the base unit 36.

[0029] Figures 3A, 3B, 4A and 4B illustrate the earmold 12 as having an earmold tip 18. As shown, the earmold tip 18 has a mushroom shaped design. Such a design can aid in securing the modular hearing aid 10 within a user's ear. The mushroom shaped design can also provide comfort, ease of insertion and sound attenuation. The mushroom shaped tip can be made from a low modulus, low durometer material, such as silicone. Such a material allows the mushroom shaped tip to be flexible and compliant. The earmold tip 18 having a mushroom shaped design can be used with all embodiments of the modular hearing aid 10.

[0030] Figure 5 illustrates an alternate embodiment of the modular hearing aid 10 where the replaceable earmold 12 is integrated with a shell 48 having a battery 22 and receiver 26. Some hearing aid shapes would benefit from a better design if the shell 48 was replaceable. For example, most in-the-canal (ITC) and completely-in-the-canal (CIC) hearing aids have receivers which are acoustically and mechanically sealed to a shell. These hearing aids would realize the benefits of a replaceable receiver section only if the shell 48 was replaced. By integrating the earmold 12 with a shell containing a battery 22 and receiver 26, in this embodiment, the shell 48 is replaceable with the earmold 12.

[0031] This embodiment can have a base unit 36 having a microphone 30 and electronics 28. The base unit 36 can have base unit connectors 40 which allow for electrical contact between a receptacle section 42 and the base unit 36. In a preferred embodiment, power (battery) and signal (receiver) conductors are required. The earmold 12 integral with the shell 48, having the battery 22 and receiver 26, can be mechanically or frictionally attached to the non-replaceable base unit 36. The mechanical attachment can be a snap fit.

[0032] Figures 6 and 7 show embodiments of the hearing aid 10 where a receiver 26 is incorporated with the earmold 12. In one embodiment, shown in Figure 6,

the earmold 12 and receiver 26 are incorporated as an integral and replaceable unit but the earmold 12 is defined as a tip section 18 only. In another embodiment, shown in Figure 7, the earmold 12 is defined as a tip 18 and a sleeve 20. In either embodiment, the modular hearing aid 10 can have a base unit 36 which can include a shell 50, a microphone 30, a battery 22 and electronics 28.

[0033] The advantages of having a replaceable earmold 12 and receiver 26 have been described above. In this embodiment, the battery 22 within the base unit 36 can be replaced, but is not integrated into the earmold 12. The earmold 12 integral with the receiver 26 can be mechanically or frictionally attached to the base unit 36. The receiver 26 can have contacts 32 which can provide an electrical connection to the base unit 36 and allow the passage of signal from the base unit 36 to the receiver 26. The contacts 32 of the receiver 26 can also be used to retain the integrated earmold 12 to the base unit 36.

[0034] In another embodiment, the base unit 36 can have a base unit shell 50 and an earmold shell 52 where the earmold shell 52 can be integrated with the earmold 12, as shown in Figure 8. In this embodiment, the integrated earmold 12 and shell 52, as well as the battery 22, can be replaced. The battery 22, however, is preferably not integrated with the earmold 12 and shell 52. The integrated earmold 12 and shell 52 can also include a replaceable receiver 26. The hearing aid 10 can also have a base unit 36 which can include a microphone 30, electronics 28 and a shell 50. The base unit shell 50 and the earmold shell 52 include an attachment mechanism which allows each shell to be joined together. The attachment mechanism can include a flexible integral snap having two joinable portions, a first portion molded to the base unit shell 50 and a second portion molded to the earmold shell 52. The attachment mechanism can also include screw threads between the shell 50 and earmold shell 52 to allow for the attachment of the shell 50 to the earmold shell 52. The attachment mechanism can create a seal between the base unit shell 50 and the earmold shell 52. The seal protects the internal performance of the hearing aid and minimizes internal acoustical feedback.

[0035] One advantage of this embodiment is that the user can independently replace either the integrated earmold 12 and shell 52 combination or the battery 22, as required. The battery 22 can be replaced at the end of its useful life. The integrated earmold 12 and shell 52 can be replaced for sanitary, cleanliness or performance reasons.

[0036] No electrical connections are needed between the earmold 12 and shell 52 combination. The integrated earmold 12 and shell 52 combination can be mechanically or frictionally attached to the non-replaceable base unit 36, as earlier defined.

[0037] The battery 22 and receiver 26 can have electrical connections within the modular hearing aid 10. The

battery 22 can be electrically connected to the electronics 28 and can provide power to the hearing aid 10. In a preferred embodiment, the battery 22 is held within the hearing aid 10 by a clip. The receiver 26 can also

5 be electrically connected to the electronics 28. In a preferred embodiment, the receiver 26 is electrically connected to the electronics 28 by spring conductors.

[0038] Figure 9 illustrates an alternate arrangement of a replaceable earmold 12 which allows the replacement of an integrated shell and electronics module 54 as a separate component of the earmold 12. The modular hearing aid 10, can include the earmold 12 having the shell and electronics module 54 and can also include a replaceable battery 22 connected to the shell and electronics module 54 and a non-replaceable base unit 36 having a microphone 30 and a receiver 26, which is not according to the present invention.

[0039] The battery 22 can be replaced at the end of its useful life. The shell and electronics module 54 and the earmold 12 are not integrated. The earmold 12 can be replaced separately from the shell and electronics module 54 for the purpose of cleanliness, sterility, and performance. In one arrangement the earmold 12 can be replaced on a daily basis. For peak performance and 25 maximum unit longevity, this embodiment also encompasses the replacement of the integral shell and electronics module 54. As electronic components continue to improve faster than improvements to transducer technology, it can be advantageous to replace the electronics 28 and, in particular, the hearing aid's 10 integrated circuit, independent of the transducers. This disclosure defines an integrated shell and electronics module 54 where the shell 55, in a preferred embodiment, is a convenient and protective means for mounting the electronics 28. The shell 55 can provide both electrical and mechanical connection and attachment means for the electronics 28. The shell 55 can provide the electronics 28 with a frictional attachment with the earmold 12 and with an electrical connection to the receiver 26 of the base 30 unit 36 and the battery 22.

[0040] Figure 10 shows another embodiment of the modular hearing aid 10 having a base unit 36, a replaceable earmold 12 and a replaceable shell 58 which integrates electronics 28 and a receiver 26 into a single 45 module 56. The base unit 36 can include a microphone 30 and a battery 22. In this embodiment, the earmold 12 is separately replaceable from the shell, electronics and receiver module 56.

[0041] The battery 22 and receiver 26 can have electrical connections within the modular hearing aid 10. The battery 22 in the base unit 36 can be electrically connected to the electronics 28 in the module 56. The receiver 26 can also be electrically connected to the electronics 28. In a preferred embodiment, the receiver 26 55 is electrically connected to the electronics 28 by spring conductors.

[0042] This embodiment combines the advantages of a modular hearing aid 10 having a non-replaceable base

unit 36 with the advantages of a replaceable receiver 26. The integration of the electronics 28 and the receiver 26 in a separate replaceable shell module 46 allows the user to replace the electronics 28 and receiver 26 in the hearing aid 10, simultaneously, as needed.

[0043] Figures 11, 12 and 13 show arrangements for a modular hearing aid 10 where the hearing aid 10 has a base unit 36, a replaceable shell module 46 having electronics 28 and a replaceable earmold 12 integrated with a battery 22. In each embodiment, the earmold 12 can be separately replaced for the purpose of cleanliness, sterility, and performance. The battery 22 in a hearing aid can be replaced at the end of its useful life. The battery 22 integrated with the earmold 12 can include an electrical connection to the base unit 36. By integrating the replaceable earmold 12 with the battery 22, a user can simultaneously provide himself with a sterile covering and a fresh power source for a modular hearing aid 10. The electronics 28 of the module 46 can be electrically connected to the base unit 36. The electronics 28 of the module 46 can also be electrically connected to the battery 22 integrated with the earmold 12. Also in each arrangement the shell module 46 can be replaced separately from the integrated earmold 12 and battery 22 combination.

[0044] In the arrangement of Figure 11, not according to the present invention, the base unit 36 can have a microphone 30 and a receiver 26 and the replaceable shell module 46 can have a shell 59 and electronics 28. The integration of the electronics 28 in a separate replaceable shell module 46 allows the user to replace only the electronics 28, as is needed. For example, as electronic components continue to improve faster than improvements to transducer technology, it can be advantageous to replace the electronics 28 of a hearing aid independent of the transducers.

[0045] In the embodiment shown in Figure 12, the base unit 36 can have a microphone 30 and the replaceable shell module 46 can have a shell 59, electronics 28 and a receiver 26. The integration of the electronics 28 and the receiver 26 in a separate replaceable shell module 46 allows the user to replace the electronics 28 and receiver 26 in the hearing aid 10, simultaneously, as needed.

[0046] In the arrangement of Figure 13, not according to the present invention, the base unit can have a receiver 26 and the replaceable shell module 46 can have a shell 59, a microphone 30 and electronics 28. The integration of the electronics 28 and the microphone 30 in a separate, replaceable shell module 46 allows the user to replace the electronics 28 and microphone 30 in the hearing aid 10 simultaneously, as is needed.

[0047] A method for replacing an earmold of a modular hearing aid may be as follows. In this method, a modular hearing aid having a base unit and an earmold can first be provided. Next a securing mechanism between the earmold and the base unit can be released. This allows the separation of the earmold and the base unit.

The earmold can then be removed from the base unit, discarded and replaced with a second earmold onto the base unit. This allows a user to place a clean or fresh earmold onto an existing base unit. The earmold can

5 then be attached to the base unit with the securing mechanism.

[0048] In an alternate method, the base unit of a modular hearing aid can be replaced. In this method, a modular hearing aid having a base unit and an earmold can 10 first be provided. Next a securing mechanism between the earmold and the base unit can be released. This allows the separation of the earmold and the base unit. The base unit can then be removed from the earmold, discarded and replaced with a second base unit. This 15 allows a user to replace a non-functioning or malfunctioning base unit with a working base unit. The base unit can then be attached to the ear mold with the securing mechanism.

[0049] In another method, a component of a modular 20 hearing aid can be replaced. In this method a modular hearing aid having a base unit component, an earmold component and a module component can be provided. Next, at least one securing mechanism can be released among the earmold component, base unit component 25 and module component. Next a component can be removed from the modular hearing aid, discarded and replaced. The at least one securing mechanism can then be attached among the earmold component, base unit component and module component.

[0050] Figures 14, 15 and 16 show an earmold tip 60 which has an integral mushroom shaped tip portion 62 and integral vibration isolator portion 64. The earmold tip 60 can provide comfort, ease of insertion, sound attenuation, and can help to anchor the unit in an ear.

[0051] The flexible earmold tip 60 can be constructed from a soft, low durometer material, such as silicone, and can be produced by a cast molding process for inexpensive manufacture. The soft material can provide comfort to the wearer, while generating an acceptable 35 acoustic seal between the hearing aid and ear. Because the earmold tip 60 is constructed of a low modulus, low durometer material, the earmold tip 60 provides a high level of comfort for users even when the tip 60 is located in the bony region of the ear.

[0052] Figure 16 shows an outlet port 68 which has been recessed to essentially provide a mechanism for collecting wax without clogging a sound bore 74. An integral membrane can also be deployed in the outlet port 68 to serve as a wax guard. Such a wax collection mechanism can also aid in providing comfort to a user. Also shown is a sound bore 74. The sound bore 74 connects the mushroom shaped tip portion 62 to the vibration isolator portion 64 and carries sound created by a receiver to an ear canal. The sound bore 74 has a rectangular cross-sectional shape. During manufacture of the tip 60, a spring 70 is placed around the sound bore 74 prior to the casting of the compliant material over the spring 70. The rectangular cross-sectional area of the sound bore

74 can help to maintain the position of the spring 70 during casting of the tip 60. Therefore, the sound bore 74 is surrounded not only by the spring 70 but by the compliant material which forms the tip 60. The sound bore 74 can have a cross-sectional area such that the bore 74 increases high frequency acoustical transmission from a receiver 26 to a user's ear canal. In this respect, the sound bore 74 can help match the impedance of the ear canal to the receiver 26. The sound bore 74 can also include a proximal sound bore portion 80 having a circular cross-sectional area. The circular cross-sectional area of the proximal portion 80 provides a transition between the rectangular cross-sectional area of the sound bore 74 and a receiver 26.

[0053] The mushroom shaped tip portion 62 has an optimum tip diameter 72 within the range of 6 to 12 mm, with 8 to 10 mm diameter tips fitting most individuals, while a 9 mm diameter tip being the ideal diameter. Several internal features of the mushroom shaped tip portion 62 are shown in the cut-away view of Figure 17. The mushroom shaped tip portion 62 includes a spring 70 which can be formed integral with the earmold tip 60. The spring 70 can have a stiffness value that is consistent with a desired tip flexibility. For example, the stiffer the spring, the less flexible the mushroom shaped tip portion 62 relative to the vibration isolator portion 64. The spring 70 can also act to prevent the collapse of the sound bore 74 during bending. Alternately, a stiff material can be used to surround the sound bore 74, which can allow the tip 60 to flex but not collapse. The spring 70 can have an open coil construction which permits the flow of material between coils during the manufacturing process so as to retain the spring 70 in the earmold tip 60. Finally, with respect to the spring 70, the longitudinal compressibility of the spring 70 can enhance comfort during insertion into an ear canal of a user.

[0054] The vibration isolator 64 acts to retain the earmold tip 60 in the body of a hearing aid instrument, which results in a permanently mounted tip 60. The vibration isolator 64 includes a conical shape which can help secure the earmold tip 60 within the hearing aid. Adhesives can also be used to help retain the tip in the hearing aid.

[0055] The vibration isolator 64 also acts to secure hearing aid components. The vibration isolator can include a nest 66 which houses and covers a receiver 26, as shown in Figure 18. Alternately, the receiver 26 can be partially housed and covered by the vibration isolator 64. An adhesive can be used to secure and acoustically seal the receiver to the earmold tip 60. Once the receiver 26 is seated in its nest 66, the earmold tip 60 becomes more secure because of the subassembly created by the tip and receiver 26 combination. The receiver 26 is a relatively rigid component that is confined in the vibration isolator 64 and enclosed by the hearing aid. The permanent mounting of the earmold tip 60 to the hearing aid can alleviate the potential hazards associated with tip detachment in the ear.

[0056] The vibration isolation properties of the earmo-

ld tip 60 are due largely to the compliance of the tip material. Because of the compliance, the vibration isolator 64 can mechanically decouple the receiver 26 from the hearing aid. To illustrate, the receiver 26 includes a di-

5 aphragm such that when the receiver 26 generates sound, the diaphragm vibrates. The vibration of the diaphragm can, in turn, vibrate the receiver 26 itself. When a receiver 26 is rigidly mounted to a hearing aid, vibrations of the receiver 26 vibrate the hearing aid and its shell. Vibration of the hearing aid can create feedback within the hearing aid. Mechanical decoupling of the receiver 26 from the hearing aid can reduce this feedback phenomenon. The compliant hearing aid tip 60 absorbs vibrations from the receiver 26 caused by the vibration 10 of the diaphragm within the receiver. The tip 60 therefore isolates the mechanical vibrations of the receiver 26 from the hearing aid, thereby mechanically decoupling each portion. To obtain an effective isolator, one must consider the mass of the object, such as the receiver, 15 that is to be decoupled. By lowering the resonant frequency of receiver/nest system, the receiver vibrations are highly attenuated.

[0057] In addition to vibration isolation, the tip 60 provides sufficient acoustic isolation to attenuate unwanted

20 feedback and associated oscillations during operation. Part of the isolation is obtained from a seal produced by the mushroom shaped tip 62 in conjunction with a given ear canal. Such a seal can produce an external acoustic isolation from external acoustic vibration for the hearing aid. For example, the receiver of the hearing aid sends 25 sound to an ear drum. If the sound vibrations travel from the receiver and around the hearing aid and into the microphone of the hearing aid, feedback will result. A tip 60 having a mushroom shaped tip portion 62 can provide a seal which prevents sound vibrations from traveling around the hearing aid to the microphone. The feedback path from the output of the receiver to the microphone is attenuated by the mushroom shaped tip.

[0058] To prevent the sound from the receiver 26 from 30 leaking internally to the microphone 30, soft material, by way of the isolation nest 66, can completely surround the receiver thereby attenuating internal acoustic vibrations transmitted from the receiver 26 to the microphone 30. Without the presence of acoustic isolation of the receiver 26, as the receiver 26 produces sound, the sound can leak from the output of the receiver 26, around the receiver 26, and back to the microphone 30 within the hearing aid itself. Such a sound leak can create feedback oscillations. Surrounding the receiver 26 with a 35 compliant material, such as the nest 66, can eliminate any spaces around the receiver 26 through which sound can travel. The compliant material surrounding the receiver 26 acts as a gasket to provide a good acoustic seal for the receiver, thereby providing internal acoustic isolation. Alternately, to create internal acoustic isolation, the soft material could partially enclose the receiver, with an adhesive used to complete the seal.

[0059] Figures 19 and 20 show the tip 60 mounted in

a hearing aid 78. Figure 19 shows a hearing aid base unit having internal components, such as a battery 22, microphone 30, and electronics 28. The earmold tip 60 is mounted within the base unit such that the receiver can electronically connect to the electronics 28. Figure 20 depicts an assembled hearing aid 78. The hearing aid 78 includes a hearing aid base unit 80 and a tip 60. The tip 60 is clamped between two half-shell portions of the hearing aid base unit 80.

[0060] Mechanical feedback in a hearing aid can also be reduced by potting the inside of hearing aid with a material that increases the mass of the hearing aid. Potting the inside of the hearing aid can embed the components of the hearing aid, such as a receiver, a microphone, electronics, controls and a battery, within a material. The potting material can form an acoustical barrier inside the hearing aid between the receiver and the microphone. The material can also be used to pot a portion of the inside of the hearing aid base unit. The potting material used to reduce mechanical and acoustical feedback can be epoxy, for example.

[0061] An increase in mass of the hearing aid can help to attenuate vibrations created by the receiver during operation, thereby preventing the vibrations from being conducted to a portion of the hearing aid shell near the hearing aid microphone and causing mechanical feedback oscillation. The increase in mass can also reduce acoustical feedback by creating a blocking wall so as to prevent the acoustical vibration energy created by the receiver from traveling through air inside the hearing aid housing. The potting material can also increase the stiffness of the base unit, thereby raising its resonant frequencies above the typical feedback oscillation frequency range to reduce feedback in the hearing aid.

[0062] Potting the inside of a hearing aid to prevent the transmission of mechanical vibration and acoustical energy has not been performed previously. A hearing aid which is potted renders any required repairs on the hearing aid as very expensive, since the repairer would have to work through the potting material to reach the components to be repaired or replaced. Therefore, by virtue of a hearing aid being potted, the hearing aid must be disposed once a component of the hearing aid has failed. If the hearing aid is intended to be disposable, potting is an effective solution to feedback problems.

[0063] Figures 21-24 illustrate a disposable hearing aid, which is not according to the present invention having a compliant tip 90. The disposable hearing aid with a compliant tip 90 includes a hearing aid 92 having a hard shell, which contains the battery and all of the electronics, and a compliant tip 94 that can penetrate deep into an ear canal and is attached to the hearing aid 92 by a flexible core 96.

[0064] The compliant tip 94 can consist of many layers of thousands of tiny fingers 98 arranged around a flexible core 96, as shown in Figures 21 and 22. The fingers 98 can be made from a soft elastomer such as silicone rubber, for example. The fingers 98 can also be

formed into a round or rectangular cross section, shown in Figure 22. When the fingers 98 of the tip 94 slide into an irregular shaped ear canal, the fingers 98 can bend, twist, or interleave to form an acoustic seal to separate

5 an inner and outer area of the ear canal. The flexible core 96 at the center of the fingers 98 of the tip 94 is hollow, thereby forming a sound bore 100. The sound bore 100 allows amplified sound to pass through the tip 94 to the inner ear. The flexible core 96 can accommodate any angle change in the ear canal while the fingers 98 can accommodate any size or shape change in the ear canal.,

[0065] The compliant tip 94 can also consist of a fluid filled bladder 102 around the flexible center core, as

15 shown in Figures 23 and 24. The bladder can have a donut-like shape. The fluid within the bladder 102 can be air or liquid, for example. If the bladder 102 is filled with air, when the tip 94 is placed within an ear canal and the tip 94 is deformed, the air can compress and force the thin bladder walls 104 to stretch to accommodate various ear canal shapes and sizes. If the bladder 102 is filled with a liquid, such as water, the water will flow to accommodate shape changes of the canal. However, when liquid is used to fill the bladder 102, the walls

20 104 of the bladder 102 must be flexible enough to stretch to accommodate size changes. The liquid can contain a jelling agent to prevent any feeling of liquid sloshing in the user. The fluid filled bladder 102 can fill a void smoothly, rather than buckle like solid rubber rings when 30 the rings enter a cavity which is much smaller than the diameter of the ring.

[0066] While this invention has been particularly shown and described with references to preferred embodiments thereof, it will be understood by those skilled

35 in the art that various changes in form and details may be made therein without departing from the scope of the invention encompassed by the appended claims.

40 Claims

1. A modular hearing aid (78) comprising:

45 a base unit (80) adapted to contain any of a microphone (30), a battery (22), electronics (28) and controls; and
an earmold (60) removably attached to the base unit, the earmold comprising a compliant tip portion (62), and a retention mechanism for connection to the base unit such that the earmold can be connected to the base unit or removed from the base unit and replaced after use; the hearing aid characterised in that:

55 the earmold has a receiver (26) contained therein; and
the earmold is configured to form an acoustic seal in the ear canal.

2. The modular hearing aid (78) of claim 1, wherein the receiver (26) is contained in a nest (66) in the earmold.
3. The modular hearing aid (78) of claim 1, wherein the compliant tip portion (62) is mushroom shaped.
4. The modular hearing aid (78) of claim 1, wherein the acoustic seal is formed proximate to the tympanic membrane.

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Patentansprüche

1. Modulare Hörhilfe (78), aufweisend:

eine Grundeinheit (80), geeignet jedes von einem Mikrofon (30), einer Batterie (22), Elektronik (28) und Regler zu enthalten, und

einer Ohrform (60), die entfernbar an die Basis-
einheit angebracht ist, wobei die Ohrform ein
nachgiebiges Endteil (62) und einen Rückhal-
termechanismus zum Anschluss an die Basis-
einheit aufweist, so dass die Ohrform an die Ba-
siseinheit angeschlossen und nach Gebrauch
von der Basiseinheit entfernt und ersetzt wer-
den kann, wobei die Hörhilfe **dadurch gekenn-
zeichnet ist, dass**

die Ohrform einen Empfänger (26) auf-
weist, der darin enthalten ist, und
die Ohrform so gestaltet ist, dass sie im
Ohrkanal eine akustische Abdichtung bildet.

2. Modulare Hörhilfe (78) nach Anspruch 1, **dadurch gekennzeichnet, dass** der Empfänger (26) in ei-
nem Nest (66) in der Ohrform enthalten ist.
3. Modulare Hörhilfe (78) nach Anspruch 1, **dadurch gekennzeichnet, dass** das nachgiebige Endteil (62) pilzförmig ist
4. Modulare Hörhilfe (78) nach Anspruch 1, **dadurch gekennzeichnet, dass** die akustische Dichtung in
der Nähe des Trommelfells gebildet ist.

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et un mécanisme de retenue pour la liaison à l'unité de base, de telle sorte que l'embout auriculaire peut être relié à l'unité de base ou retiré de l'unité de base et remplacé après utilisation ; l'appareil auditif étant **caractérisé en ce que :**

l'embout auriculaire présente un récepteur (26) contenu à l'intérieur de celui-ci ; et l'embout auriculaire est configuré pour former un joint acoustique dans le canal auri- culaire.

2. Appareil auditif modulaire (78) selon la revendica-
tion 1, dans lequel le récepteur (26) est contenu
dans une empreinte (66) dans l'embout auriculaire.
3. Appareil auditif modulaire (78) selon la revendica-
tion 1, dans lequel la partie de pointe élastique (62)
est en forme de champignon.
4. Appareil auditif modulaire (78) selon la revendica-
tion 1, dans lequel le joint acoustique est formé à
proximité de la membrane du tympan.

Revendications

1. Appareil auditif modulaire (78) comprenant :

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une unité de base (80) adaptée pour contenir
un quelconque parmi un microphone (30), une
batterie (22), une électronique (28) et des dis-
positifs de commande ; et
un embout auriculaire (60) fixé de manière
amovible à l'unité de base, l'embout auriculaire
comportant une partie de pointe élastique (62),

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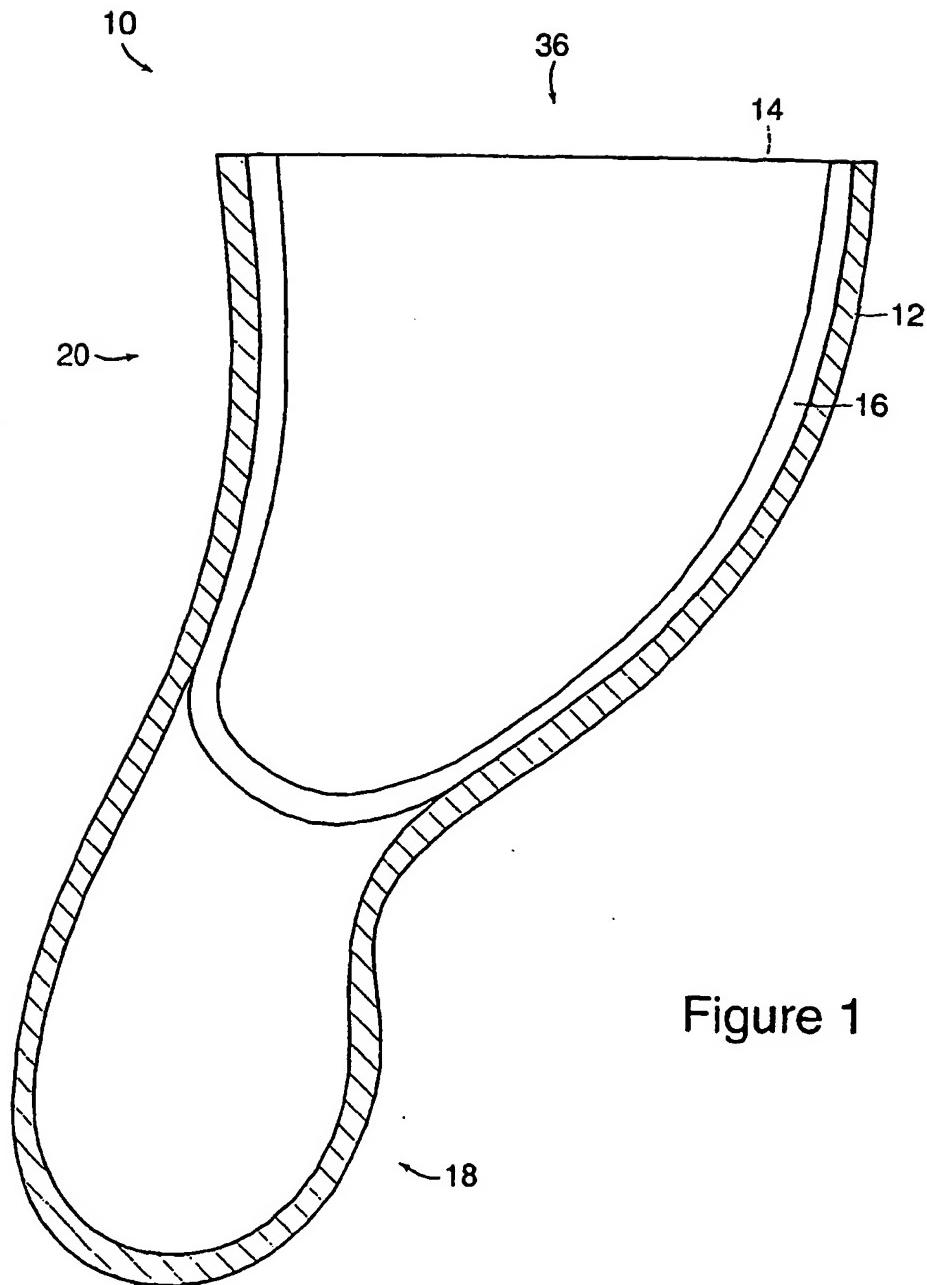


Figure 1

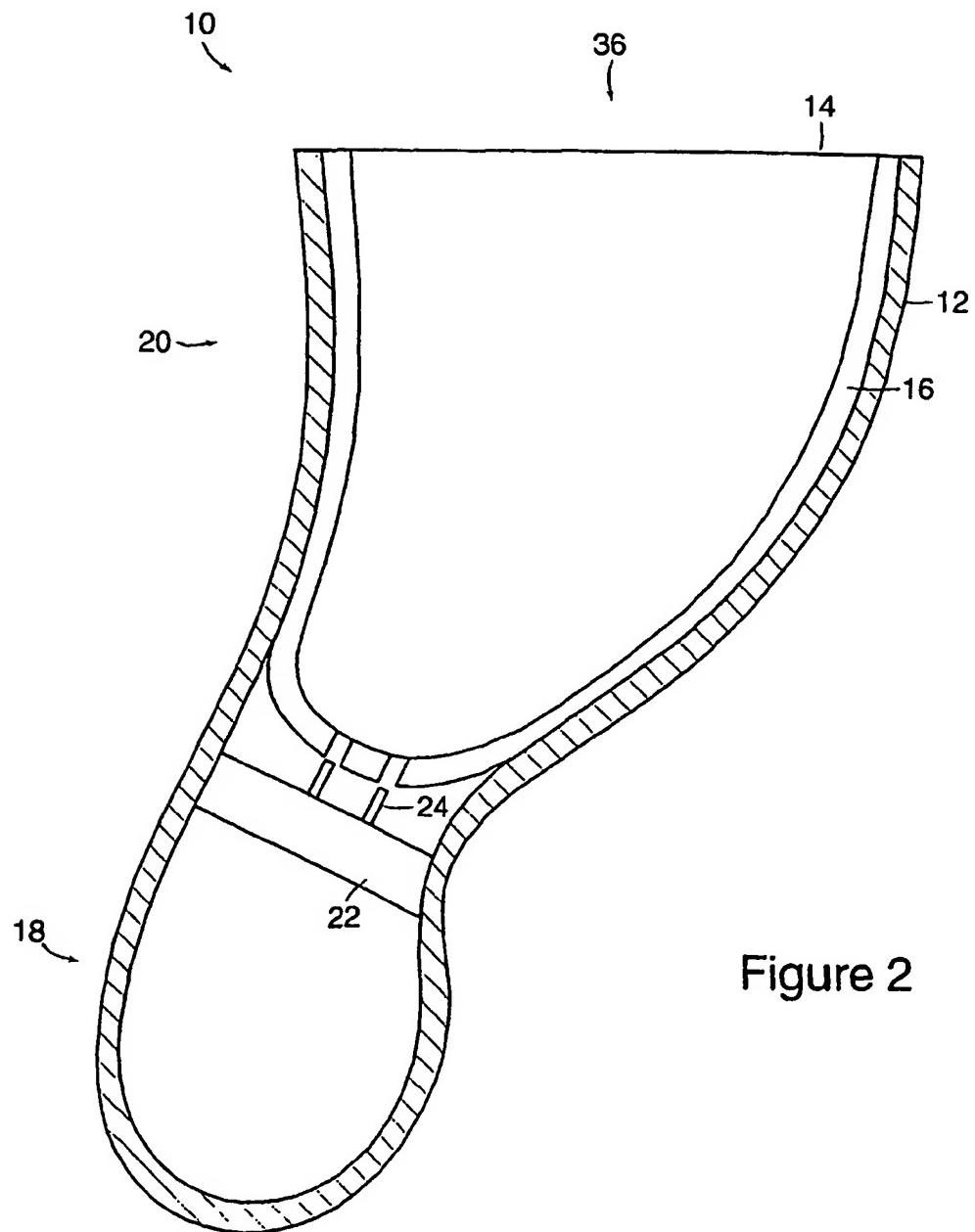


Figure 2

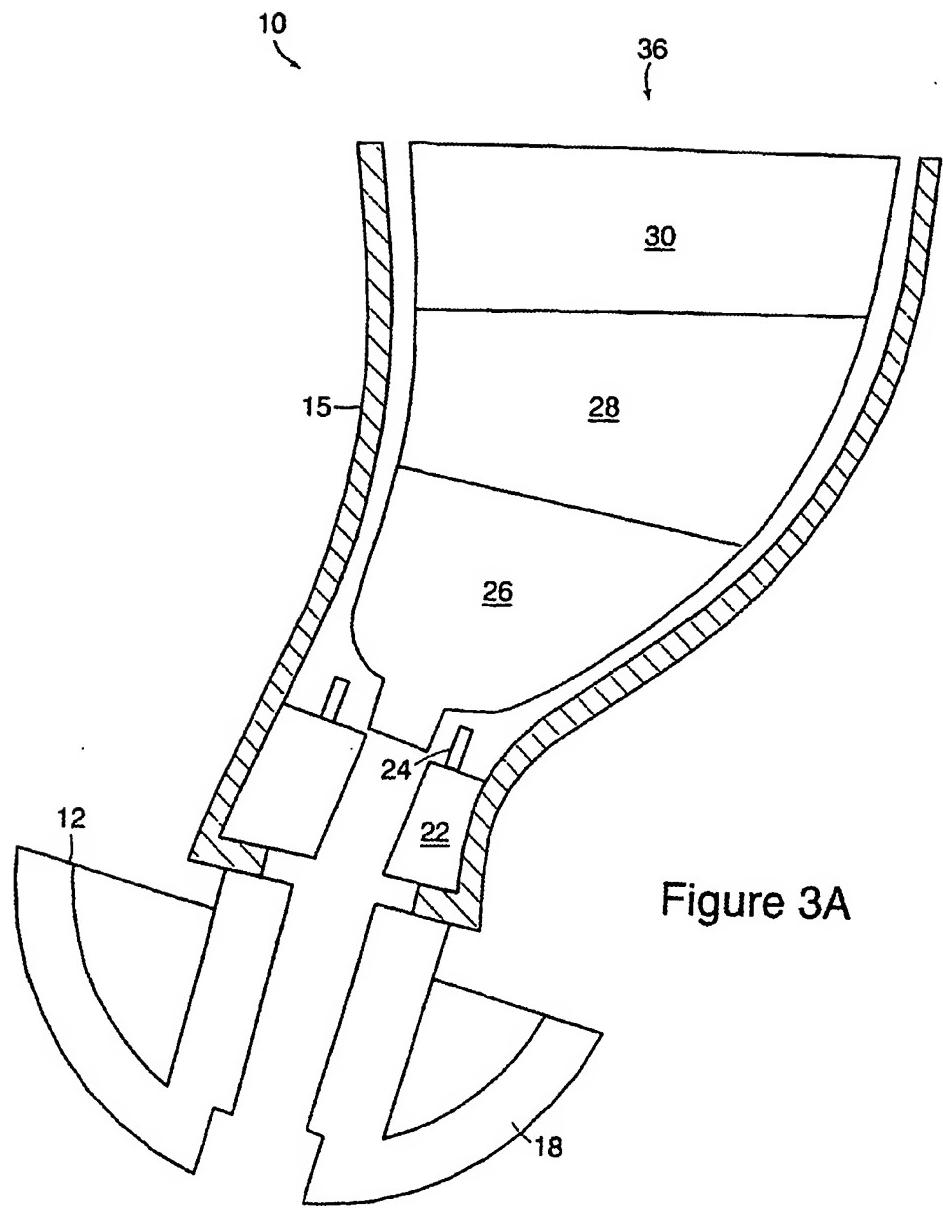


Figure 3A

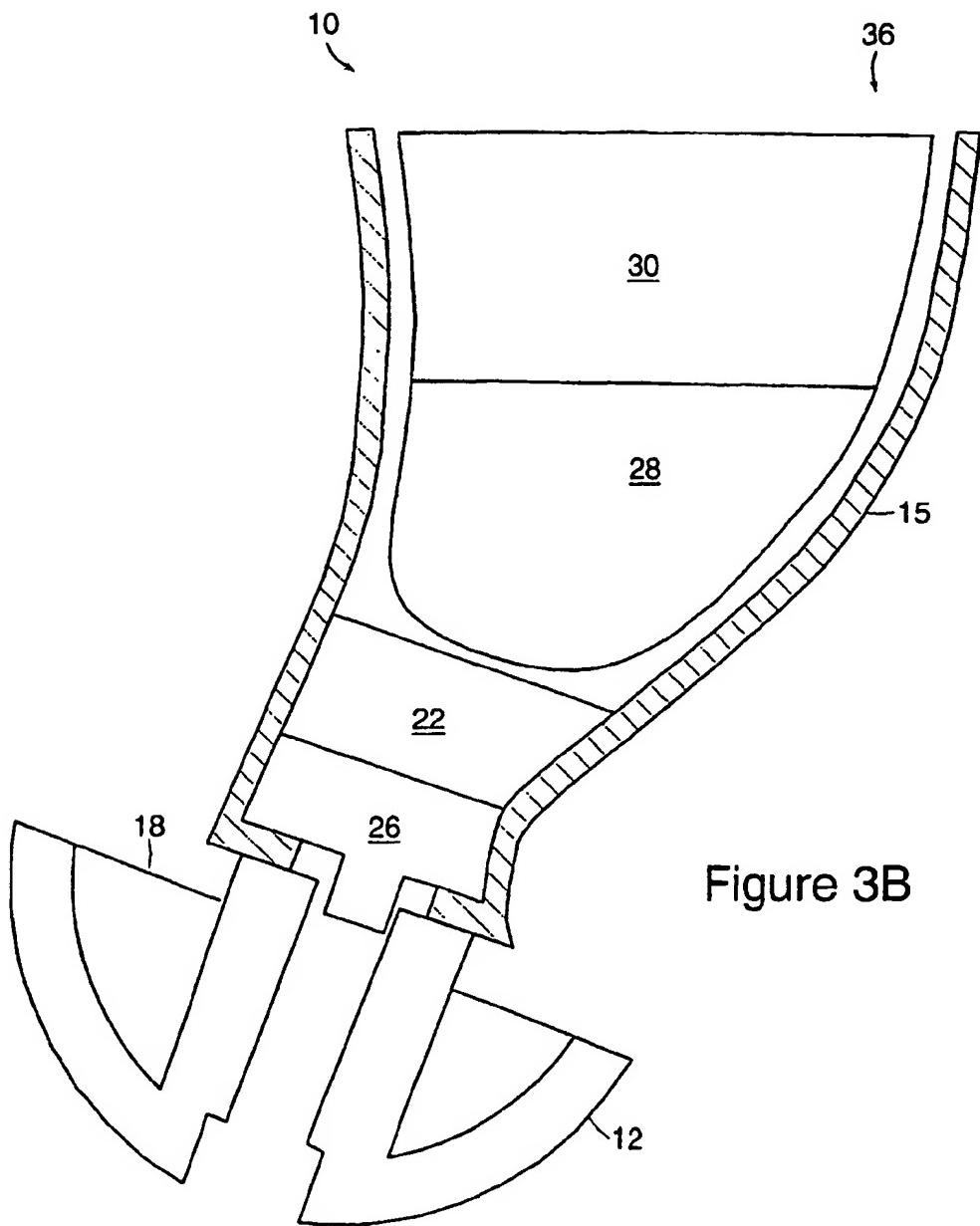


Figure 3B

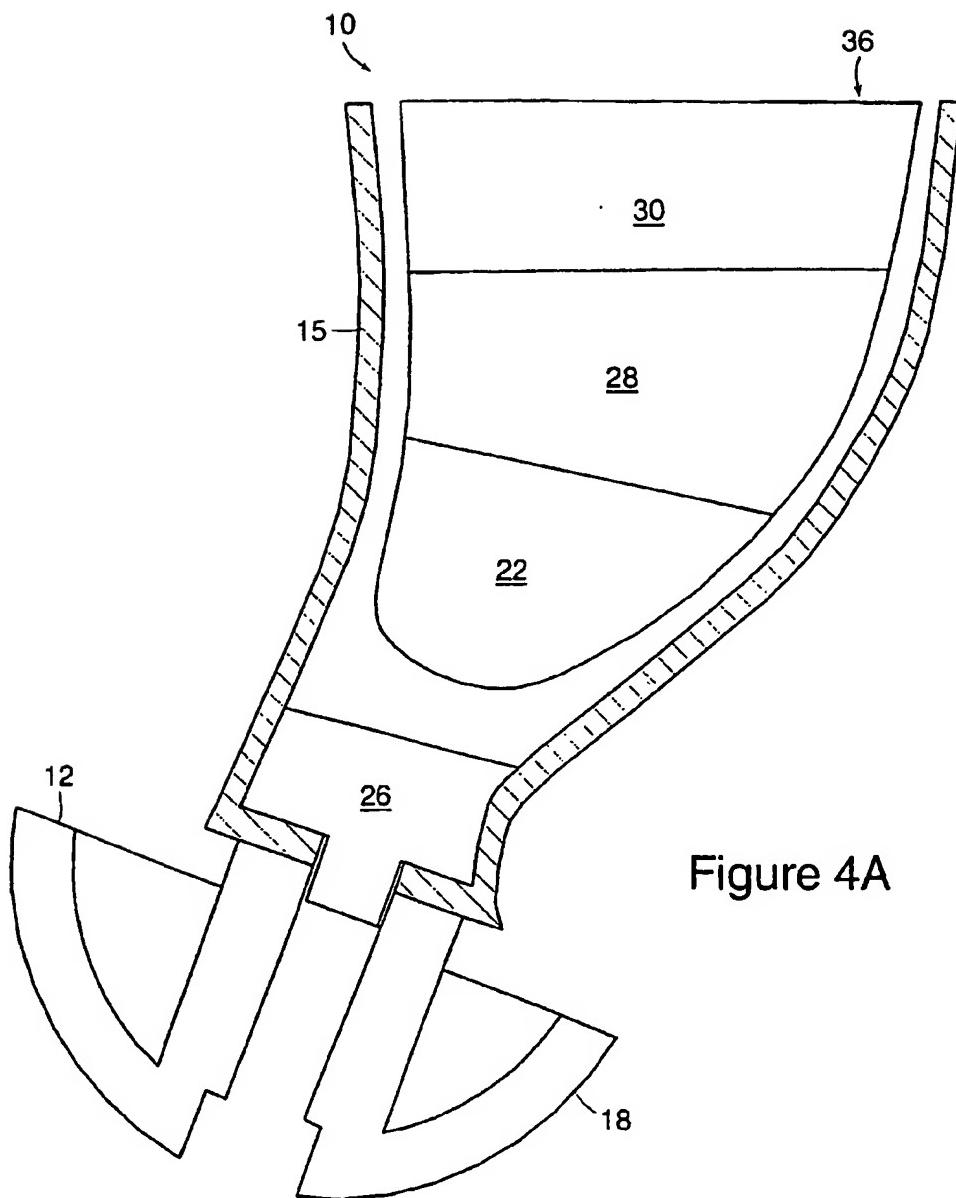


Figure 4A

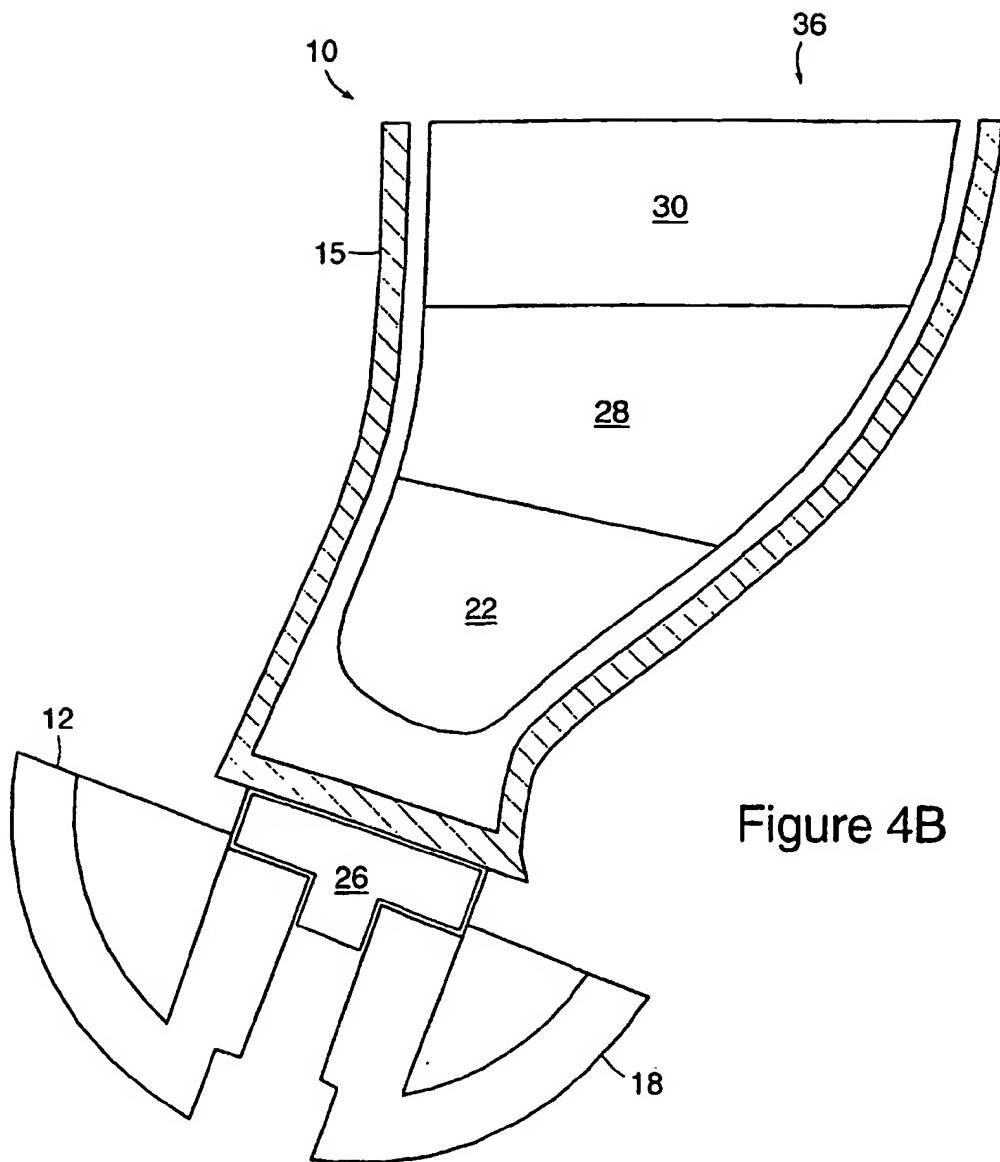


Figure 4B

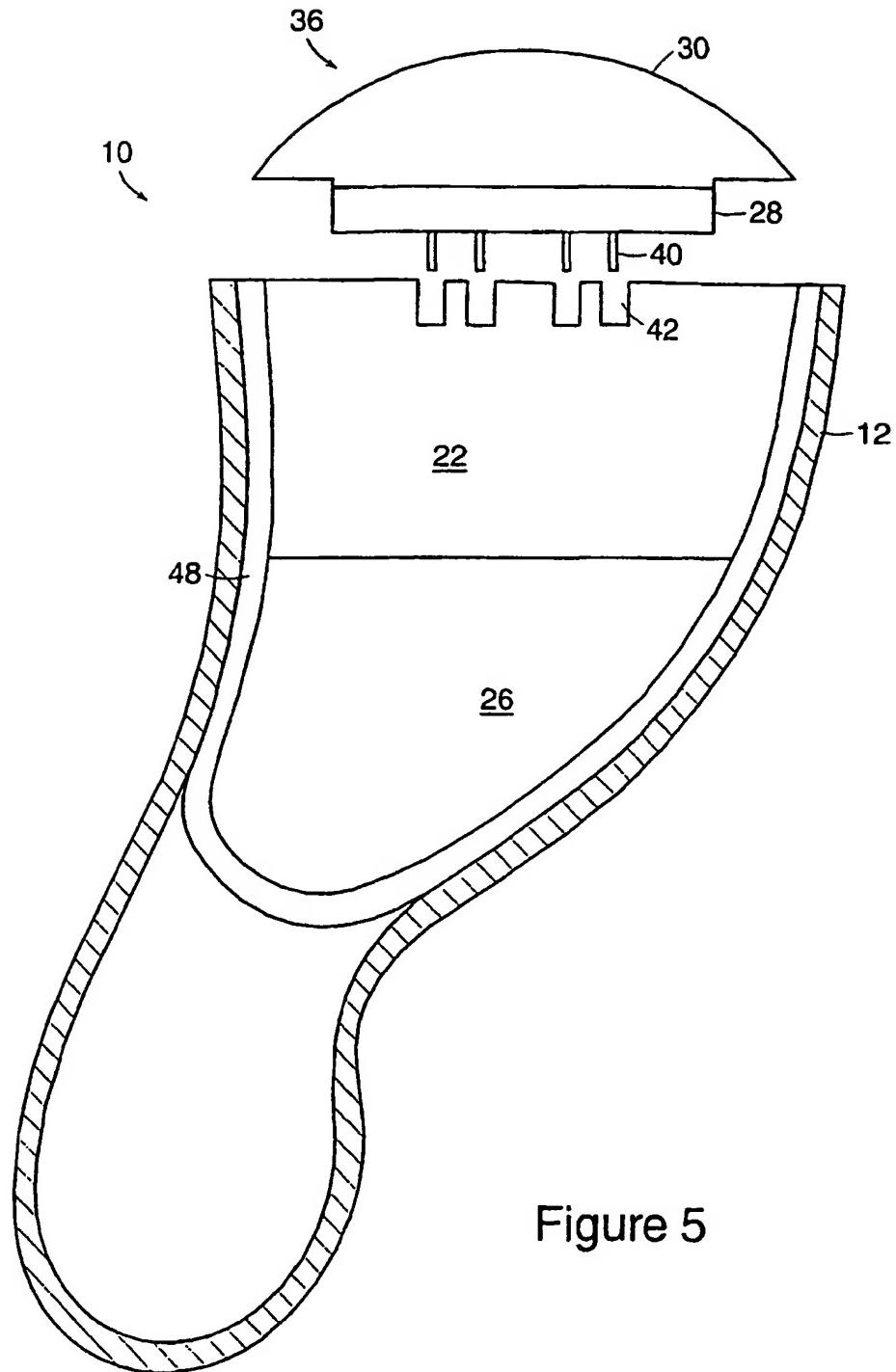


Figure 5

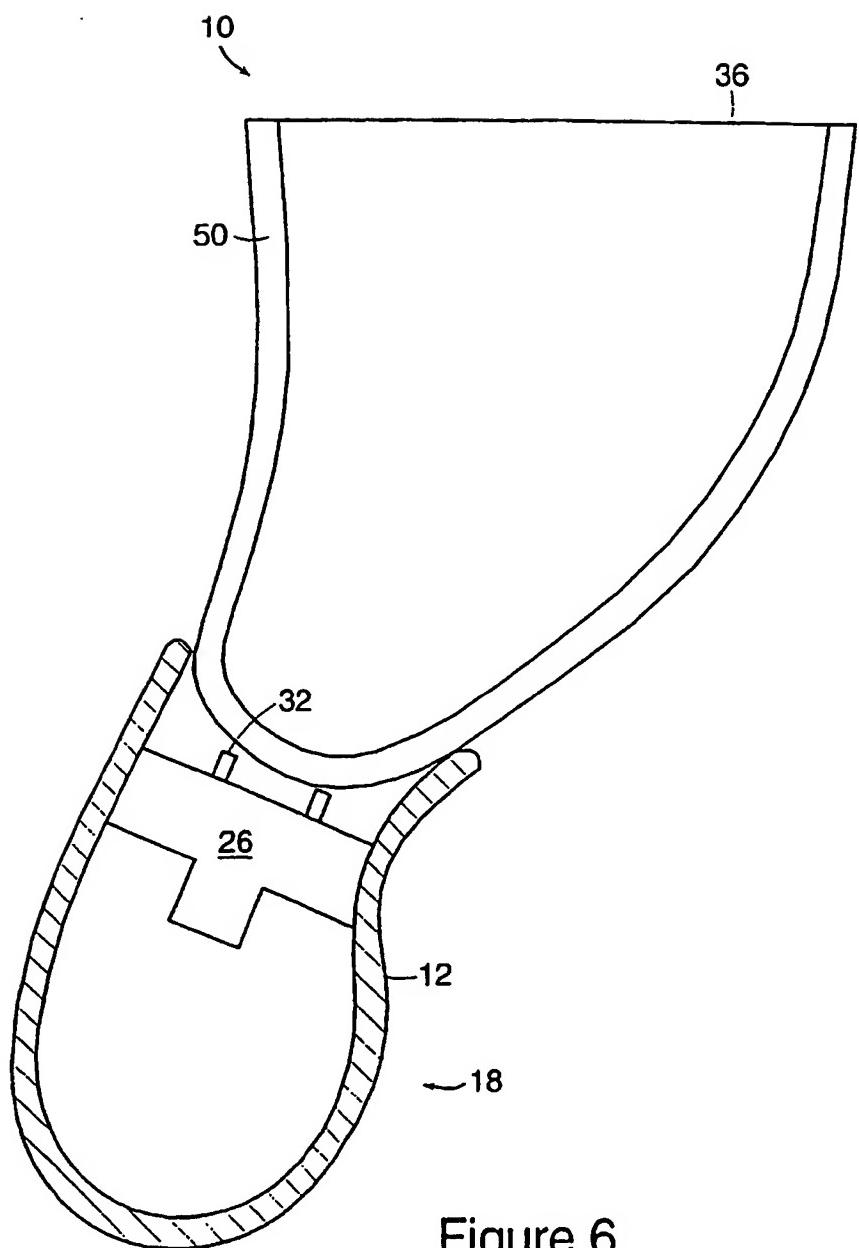


Figure 6

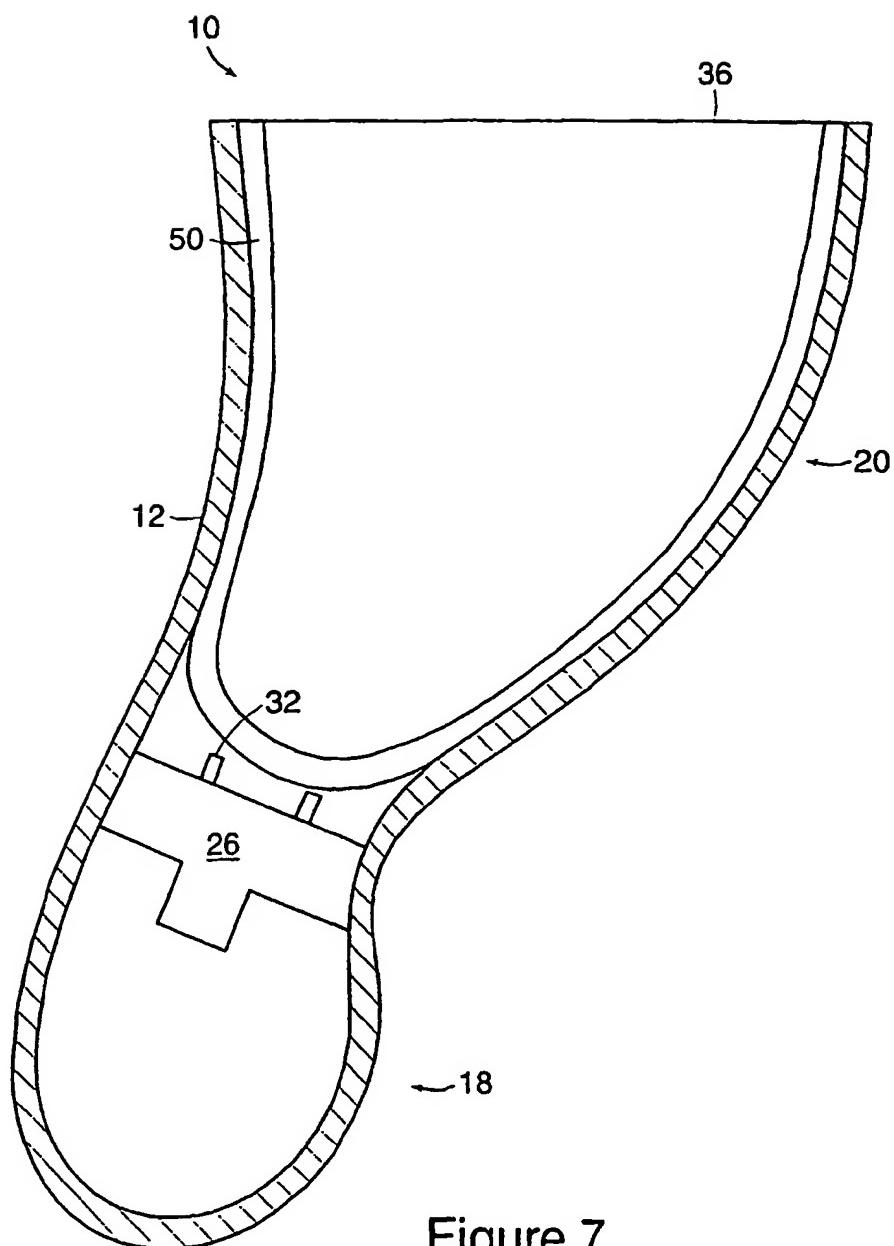


Figure 7

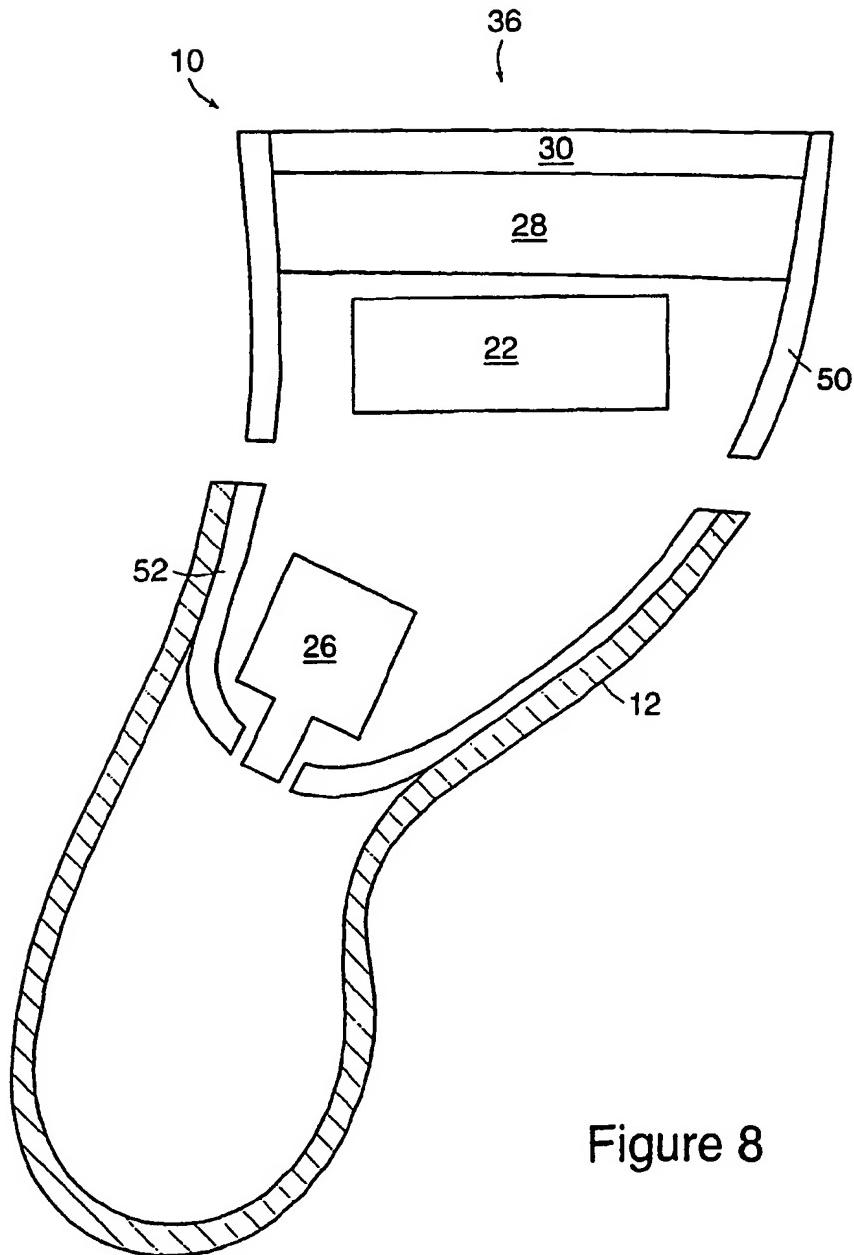


Figure 8

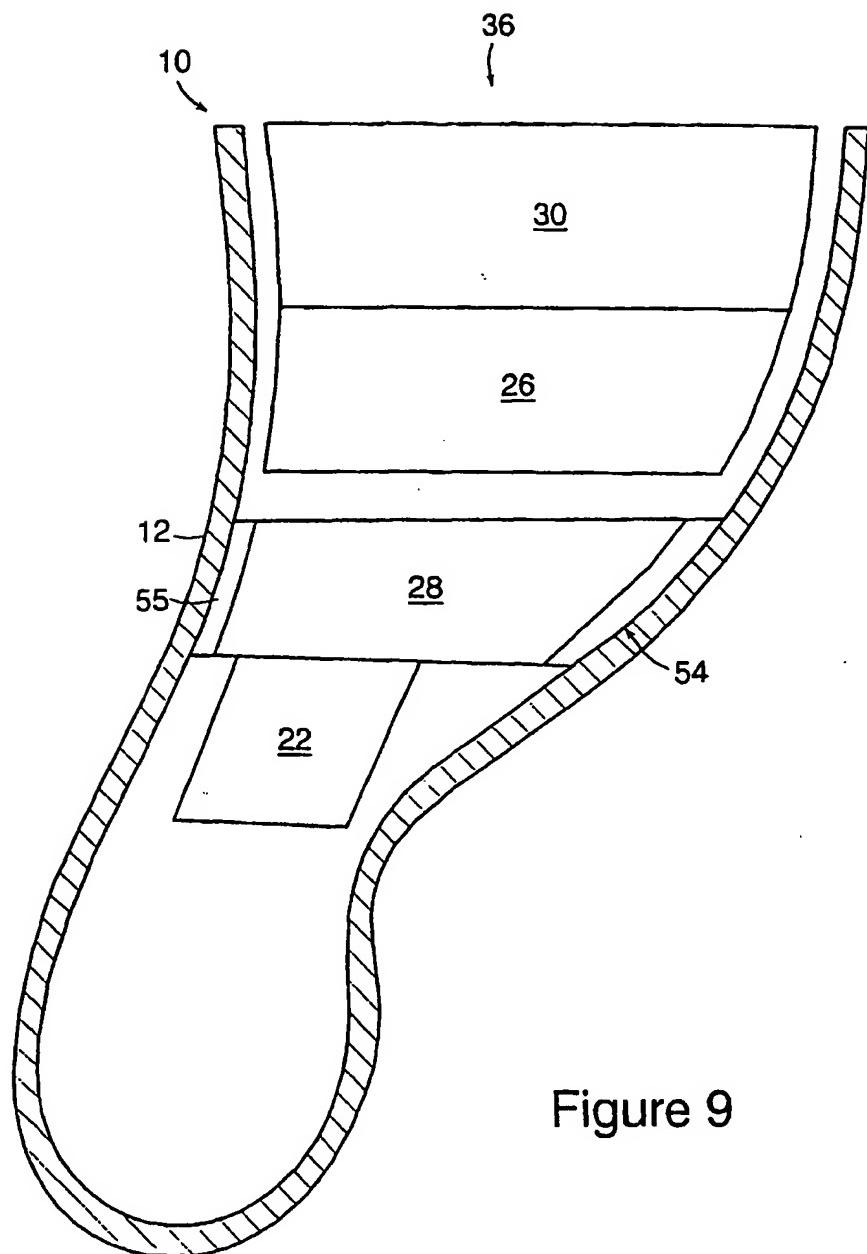


Figure 9

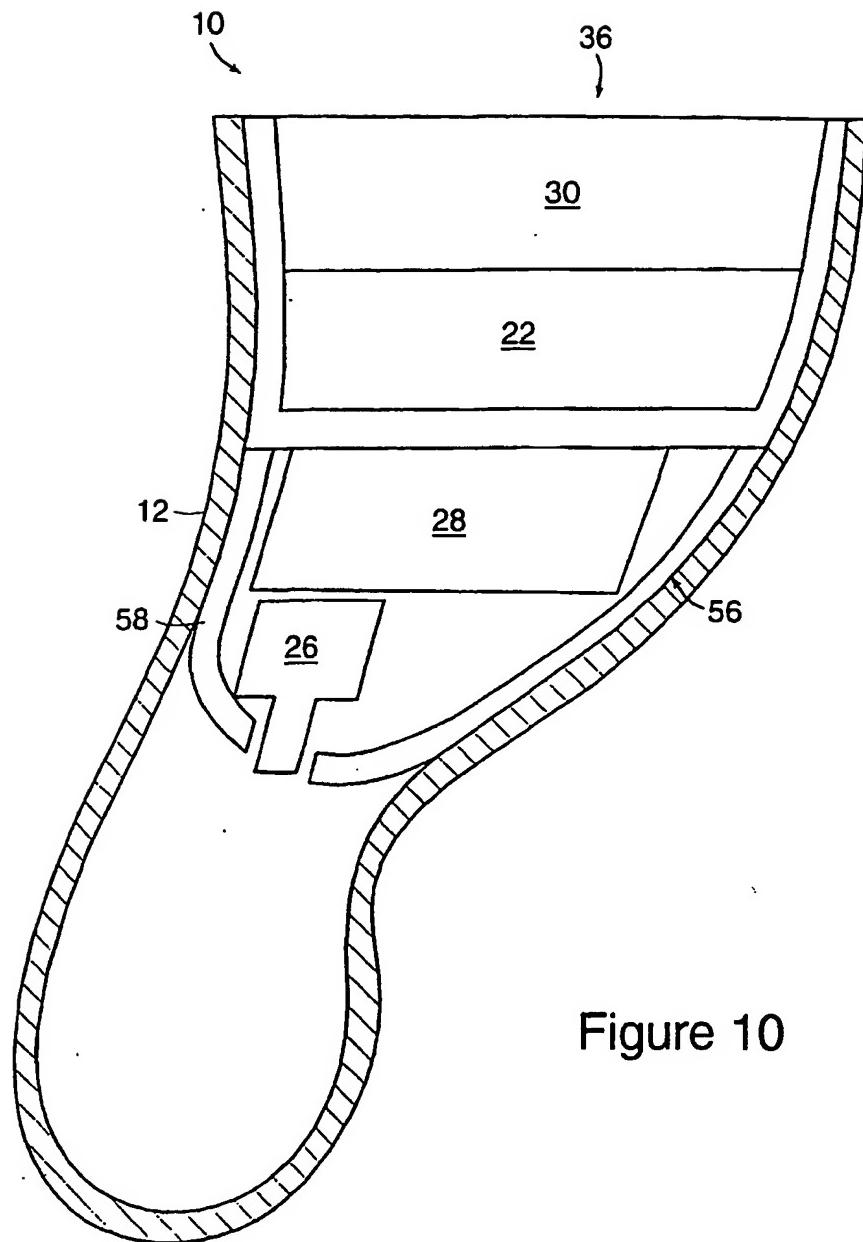


Figure 10

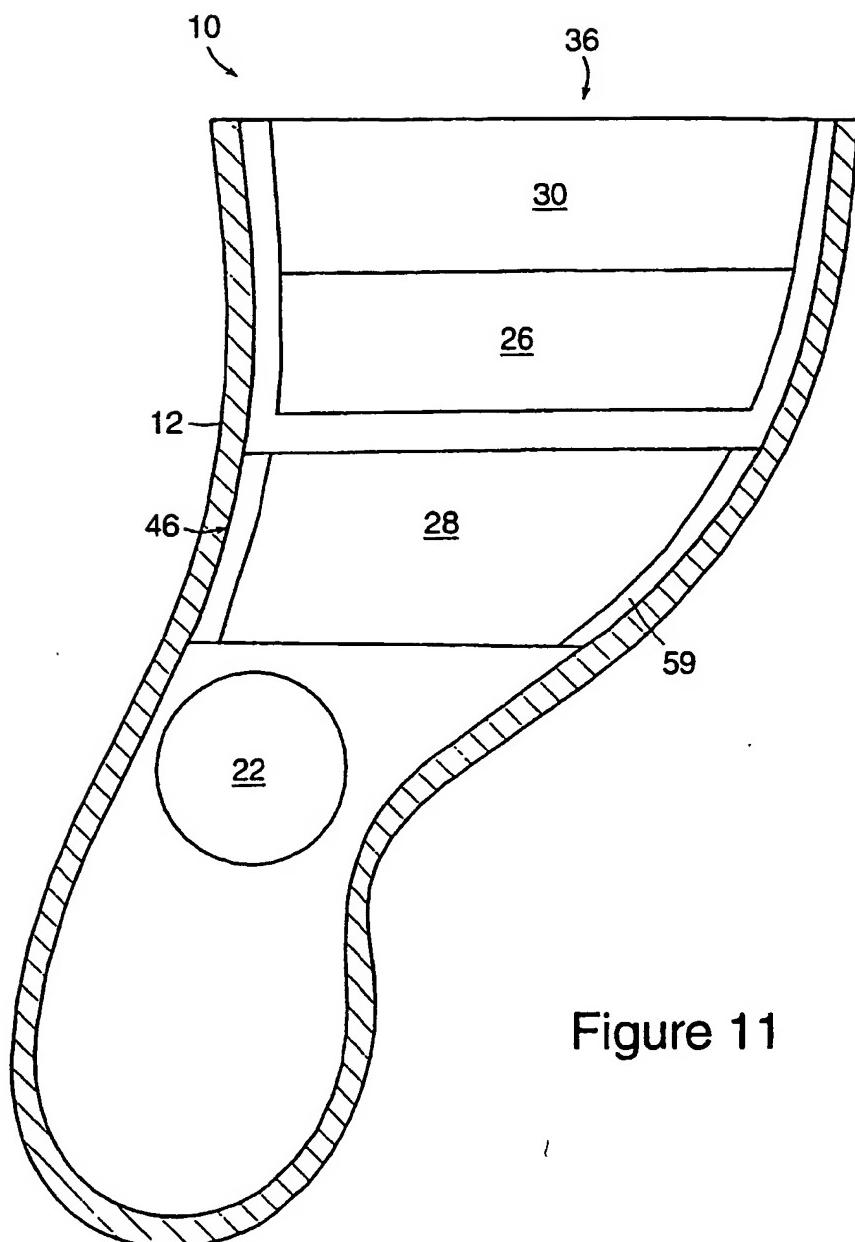


Figure 11

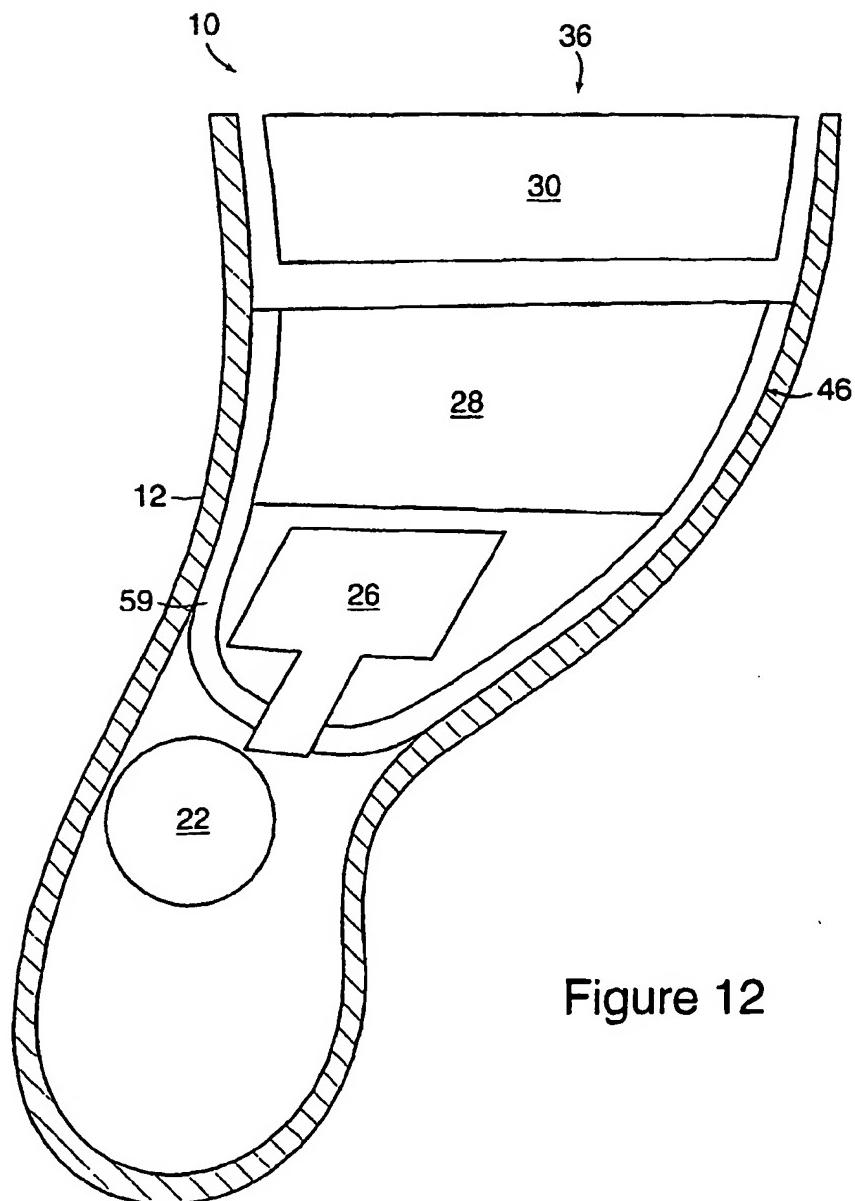


Figure 12

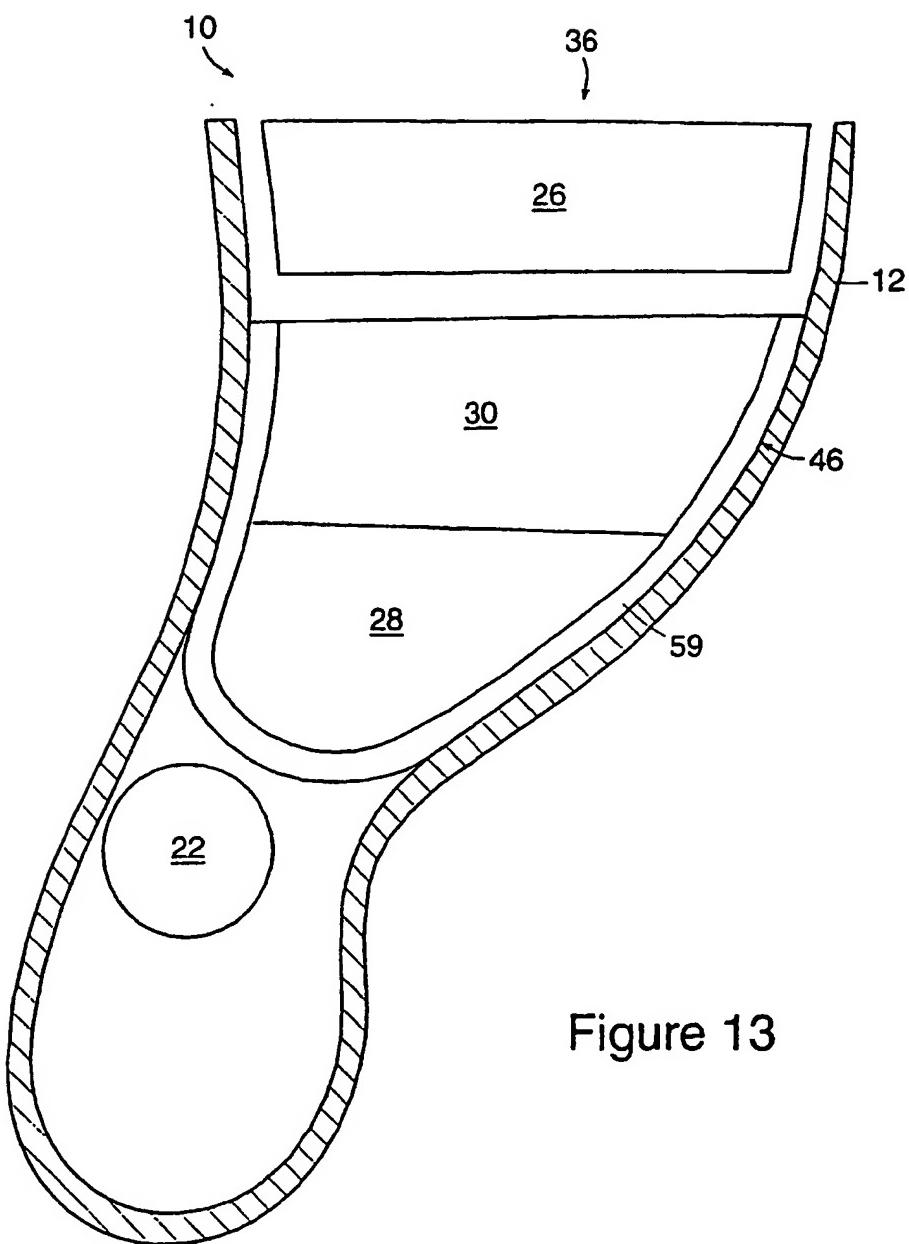


Figure 13

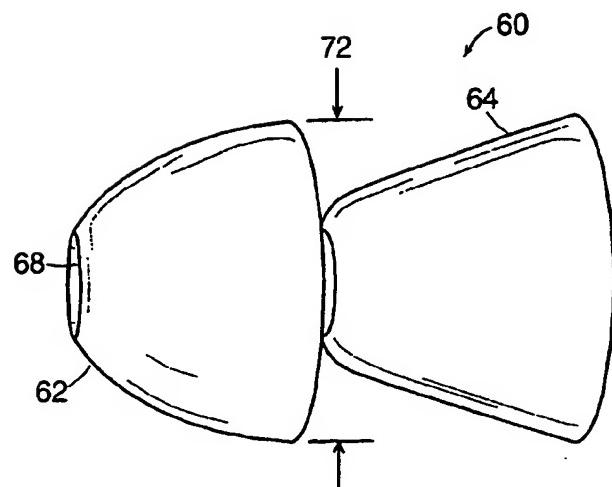


Figure 14

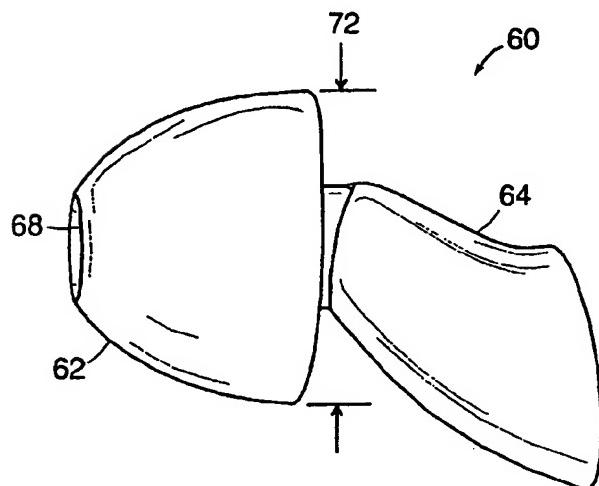


Figure 15

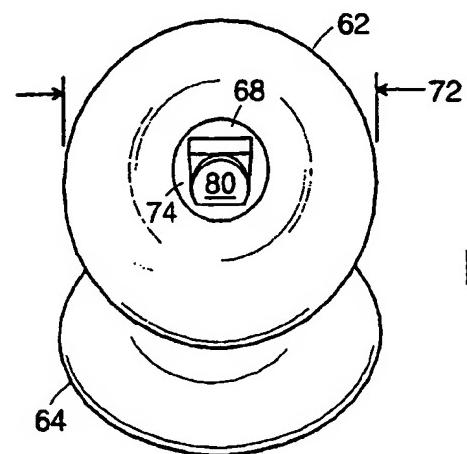


Figure 16

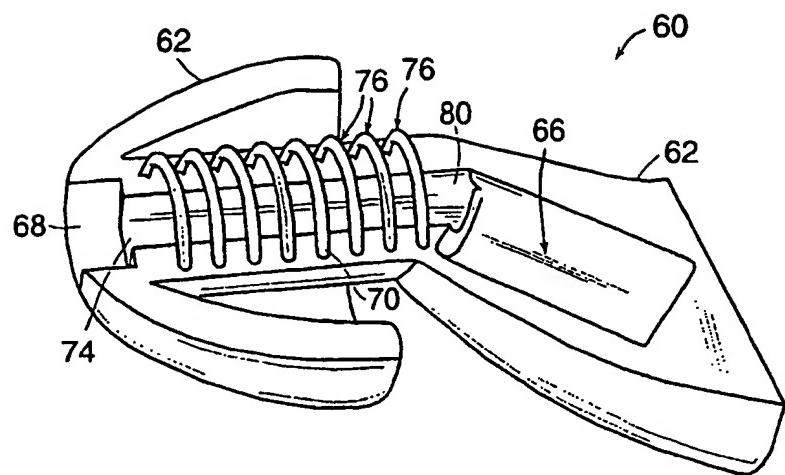


Figure 17

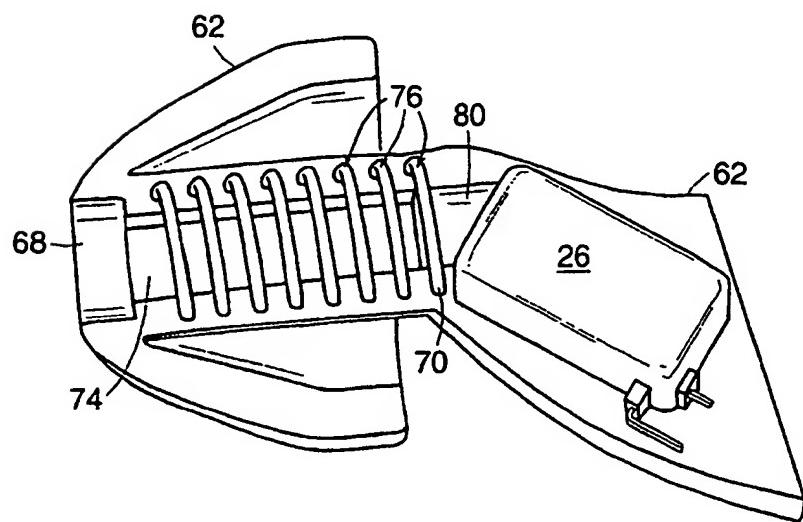


Figure 18

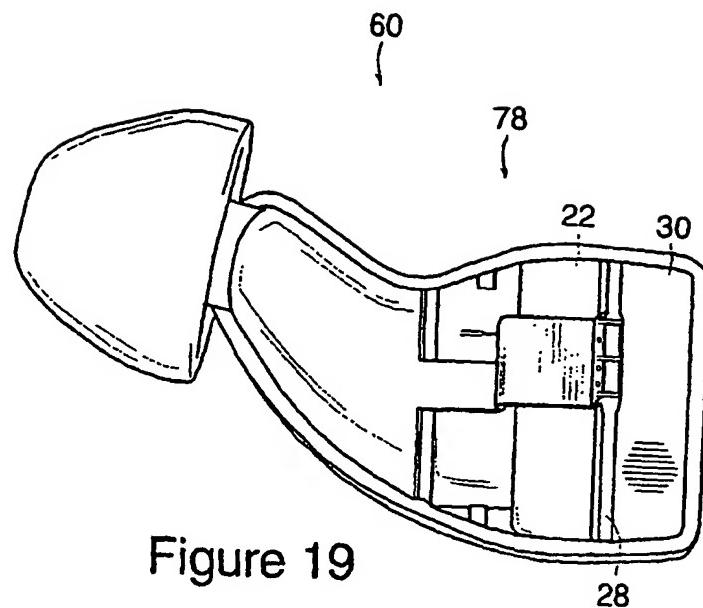


Figure 19

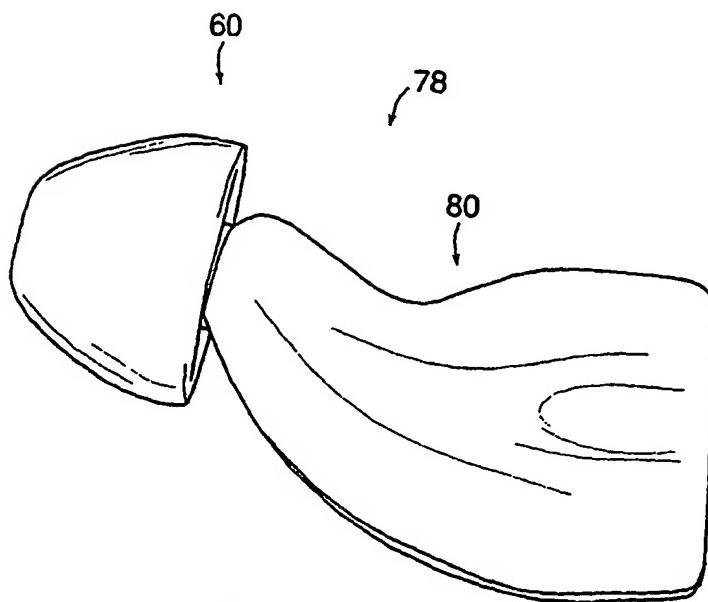


Figure 20

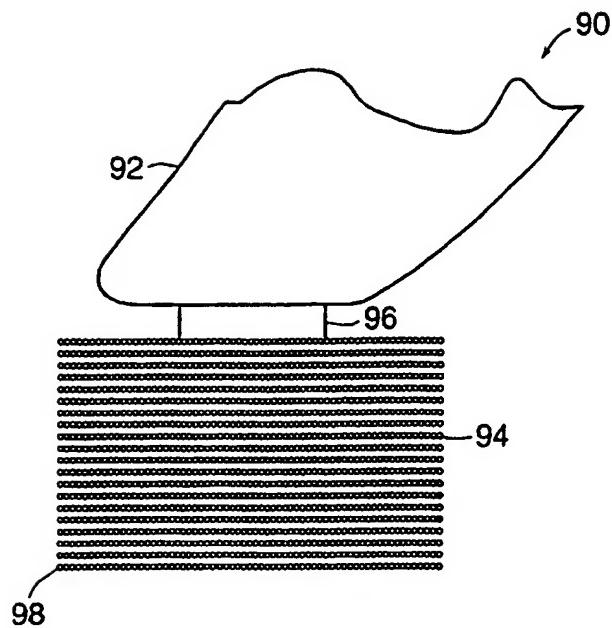


Figure 21

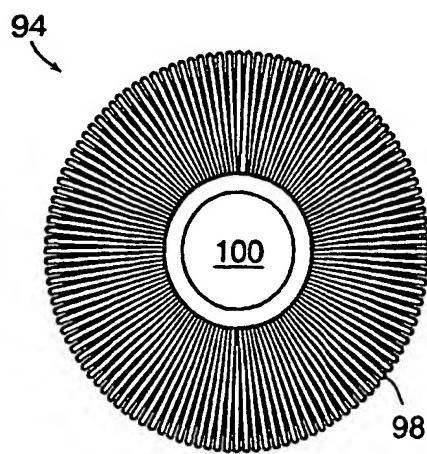


Figure 22

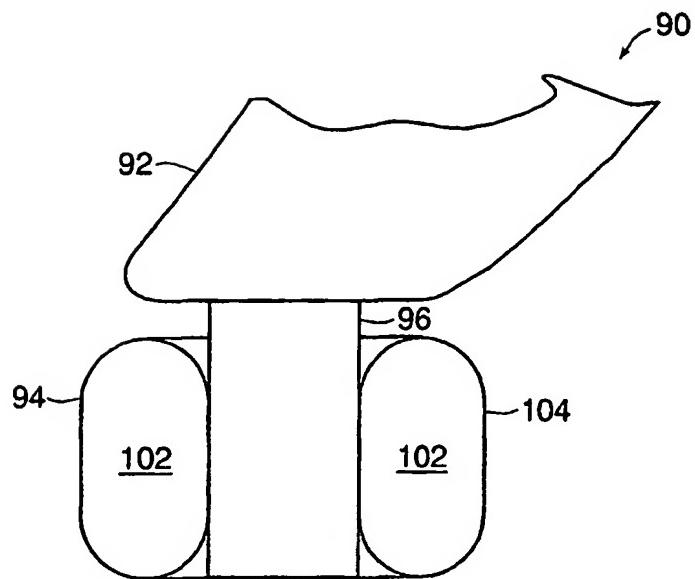


Figure 23

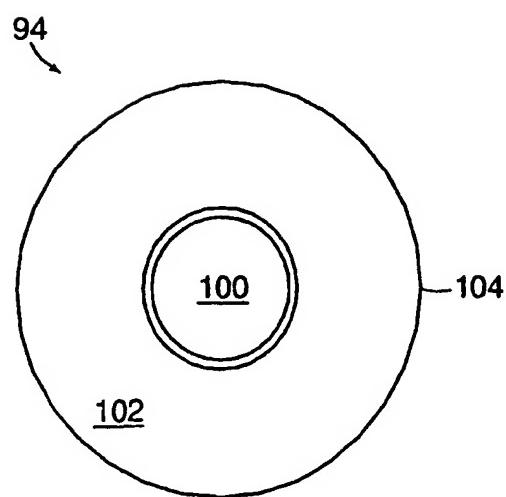


Figure 24